Modeling Blood-Vessel Walls and its Interaction with Blood Flow to the Brain

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Two Ideas

- 1. Deformation of upper layer of orbit of eye
- 2. Deformation of artery into brain while simultaneously measuring velocity, radius, blood pressure, etc.

Problem

- Modeling blood flow to brain requires dealing with complicated interaction of blood with flexible blood vessel wall
- Simulating transitional flows, wherein transition from one flow type to another, as in laminar to turbulent, is complicated enough
- But in complex geometries such as human arteries, it is further complicated.
- Adding further that such complex geometries can move or deform is even more challenging.

Specific Goal

- Wall vibration is a possible energy dissipation mechanism in transitional flows adjacent to compliant surfaces
- Investigate such combined fluid-structure interactions with a spectral element code

Brain MRI

Blood flow thru brain: too complex



Analyze flow in/out thru carotid artery

Current Models

- Fischer *et* al. model <u>transition in a stenosed carotid artery</u>: <u>http://www-unix.mcs.anl.gov/~fischer/car_trans.html</u>
- <u>Taylor</u>; *et al.* design surgical support system with FEM and MRI
- Xu used carotid artery bifurcation models reconstructed from MR scans of 3 healthy adults.

Current Models

- Blood is a complex fluid in that different types of blood cells make its modeling difficult.
- However, it could be modeled as an incompressible Newtonian fluid for the limited distance from the heart to the brain

$$\frac{\partial \mathbf{u}}{\partial t} + \mathbf{u} \quad \nabla \mathbf{u} = -\nabla p + \frac{1}{\mathrm{Re}} \nabla^2 \mathbf{u}$$

 $\nabla \mathbf{u} = 0$

Analysis

- Expand Fischer *et al*.'s work by using a compliant wall
- First step: validate compliant wall modeling with simpler 2D geometry
 - Model free surface with spectral element code
 - Model moving wall
 - Model combinations, etc.

Spectral Element Method

- Like Finite Element Method
- But with Spectral Functions
- Infinitely differentiable global functions of SEM vs. local character of FEM functions
- Adaptive mesh
- Polynomials of high and differing degrees
- Non-conforming spectral element method as described by Fischer; Patera; van de Vosse and Minev; Bernadi and Maday; with Ho's free-surface & moving wall extensions.

SEM Discretization

- Polynomial approximation for velocity two degrees higher than that for pressure
- Avoids spurious pressure modes.
- Like solving eqs. on a staggered grid where **u** and *p* are solved on different grids but coupled (e.g., via interpolation)

SEM Approach

- Temporal discretization of Navier-Stokes eqs. based on high-order operator splitting methods
 - Splitting problem into convection & diffusion
 - Some combination of integration schemes for convection operator or for time-dependent terms that may be high order
 - With some degree of polynomial for SEM discretization of diffusion terms giving high-order in space
- <u>Coupled w/SEM spatial discretization</u> to yield sequence of symmetric positive definite (SPD) sub-problems to be solved at each time step.

SEM Algorithm

• Stokes discretization based on variational form: Find (\mathbf{u}, p) in $X \times Y$ such that $\frac{1}{\text{Re}}(\nabla \mathbf{u}, \nabla \mathbf{v}) + \frac{3}{2\Delta t}(\mathbf{u}, \mathbf{v}) - (p, \nabla \mathbf{v}) = (\mathbf{f}, \mathbf{v})$

$$(\nabla \mathbf{u}, q) = 0$$

- \forall (v,q) \in *X* × *Y*, I.e., as weights in *X* × *Y*.
- Inner products: $(l,g) = \int_{\Omega(t)} l(\mathbf{x}) g(\mathbf{x}) d\mathbf{x}$

Discrete Stokes System

• Inserting SEM basis

$$f(\mathbf{x}^{k}(\mathbf{r}))|_{\Omega}^{k} = \sum_{i=0}^{N} \sum_{j=0}^{N} f_{ij}^{k} h_{i}(r_{1}) h_{j}(r_{2})$$

into

$$\frac{1}{\text{Re}}(\nabla \mathbf{u}, \nabla \mathbf{v}) + \frac{3}{2\Delta t}(\mathbf{u}, \mathbf{v}) - (p, \nabla \mathbf{v}) = (\mathbf{f}, \mathbf{v})$$

$$(\mathbf{V} \quad \mathbf{u}, q) = 0$$

yields
$$H \underline{\mathbf{u}}^n - D^T \underline{p}^n = B \underline{\mathbf{f}}^n$$
, $D \underline{\mathbf{u}}^n = 0$

where

✓ $H = A/\text{Re} + B/\Delta t$ = discrete equivalent of Helmholtz operator;

 \checkmark *A* = discrete Laplacian,

✓ B = mass matrix associated with the velocity mesh (diagonal);
 ✓ D = discrete divergence operator

Proper Subspaces

- The proper subspaces for **u**, **v**, and *p*, *q* are: $X=\{\mathbf{v}: v_i \in H^1_0(\Omega), i=1,...,d, \mathbf{v}=0 \text{ on } \partial \Omega_v\}, d=2 \text{ if } 2D...$ $Y=L^2(\Omega)$
 - L^2 is the space of square integrable functions on Ω ; $\int_{\Omega} v^2 dV = \int_{\Omega} v^2 d^3 \mathbf{r}$
 - H^1_0 is the space of functions in L^2 that vanish on the boundary (₀) and whose first derivative (¹) is also in L^2 ; $\int_{\Omega} (\partial v / \partial r)^2 dV = \int_{\Omega} (\partial v / \partial r)^2 d^3 r$
- Spatial discretization proceeds by restricting \mathbf{u} , \mathbf{v} , and p, q to compatible finite-dimensional velocity and pressure subspaces: $X^N \subset X$ and $Y^N \subset Y$

Handling Pressure

• To avoid spurious pressure modes, Maday, Patera and Rønquist, and, Bernardi and Maday suggest different approximation spaces for velocity and pressure:

 $X^{N} = X \cap \mathbf{P}_{N,K}(\Omega)$ $Y^{N} = Y \cap \mathbf{P}_{N-2,K}(\Omega)$

where

 $\mathbf{P}_{N,K}(\mathbf{\Omega}) = \{ v(\mathbf{x}^{k}(\mathbf{r})) |_{\mathbf{\Omega}}{}^{k} \in \mathbf{P}_{N}(r_{1}) \otimes ... \otimes \mathbf{P}_{N}(r_{d}), k=1,...,K \}$ and $\mathbf{P}_{N}(r)$ is space of all polynomials of degree $\leq N$

Space Dimensions

- Dimension of *Y^N* is *K*(*N*-1)^{*d*} since continuity is enforced for functions in *Y^N*
- Dimension of X^N is $dK(N+1)^d$ because
 - functions in X^N must be continuous across subdomain interfaces
 - Dirichlet bc's on $\partial \Omega_{\nu}$

Function Spaces

- <u>Velocity Space</u>: Basis chosen for $\mathbf{P}_N(r)$ is set of Lagrangian interpolants on Gauss-Lobatto-Legendre (GL) quadrature pts. in ref. domain: $\xi_i \in [-1,1], i=0,...,N$
- <u>Pressure Space</u>: Basis chosen for $\mathbf{P}_{N-2}(r)$ is set of Lagrangian interpolants on Gauss-Legendre (G) quadrature pts. in ref. domain: $\eta_i \in]-1,1[$, i=1,...,N-1
- Basis for velocity is continuous across sub-domain interfaces but basis for pressure is not

SEM Algorithm Quadrature

- Subscripts (.,.)_{GL} and (.,.)_G referred to <u>Gauss-</u> <u>Lobatto-Legendre</u> (GL) and Gauss-Legendre (G) quadrature which are:
- $\int_{-1}^{1} f(x) dx = w_1 f(-1) + w_N f(1) + \sum_{i=1}^{N} w_i f(x_i)$

Gauss-Lobatto-Legendre (GL) Quadrature

•
$$\int_{-1}^{1} f(x) dx = w_1 f(-1) + w_N f(1) + \sum_{i=1}^{n} w_i f(x_i)$$
 where
 $w_i^{GL} = \frac{2N}{(1 - x_i^2)L'_{N-1}(x_i)L'_M(x_i)} = \frac{2}{N(N-1)[L_{N-1}(x_i)]^2}$

• L_n are the *Legendre* polynomials, Gauss-Lobatto points are zeroes of L'_N or $(1-x^2) L'_N$ & at endpoints (-1,1)

$$w_{1,N}^{GL} = \frac{2}{N(N-1)}$$

Gauss-Lobatto-Legendre (GL) Quadrature

• w/error

$$E = \frac{N(N-1)^3 2^{2N-1} [(N-2)!]^4}{(2N-1)[(2N-2)!]^3} f^{(2N-2)}(\xi)$$

- for $\xi \in (-1,1)$
- The weights may also be written as

$$w_i^{GL} = \rho_i = \frac{2}{N(N+1)} \frac{1}{[L_N(x_i)]^2}$$

Gauss-Legendre (G) Quadrature

• Same as Gauss-Legendre-Lobatto <u>but</u> w/o endpoints (<u>not</u> used for prescribed function values at boundaries) and the weights are

$$w_i^G = \sigma_i = \frac{2}{(1 - x_i^2)[L_{N+1}(x_i)]^2}$$

• Where L_N are the *Legendre* polynomials, the Gauss points (interior points) are zeroes of L_{N+1}

Interpolation Polynomials

• Basis functions are Legendre-Gauss-Lobatto-Lagrange interpolation polynomials:

$$h_i = \frac{-1}{N(N+1)L_N(x_i)} \frac{(1-x^2)\dot{L_N}(x)}{x-x_i}$$

Free Surface Model

- At moving boundary $(\partial \Omega_{\sigma}(t), \text{ also traction})$ boundary) btwn fluid & other continuum is Neumann bc, $\tau_{ij} n_j = T_i = \mathbf{\tau} \cdot \hat{\mathbf{u}}_n = \mathbf{T}$, the traction.
- Surface tension (σ) modeled at this interface by adding ∫_{∂Ωσ(t)} σ κ v_i n_i dA to RHS of Stokes problem
 ∂Ω_σ(t) is for traction boundary,

 $-\kappa$ = curvature

Free Surface Model

- In 2D, $\kappa = s_{i,\xi}$,
 - $omega_i$ is a unit vector tangent to free surface segment from pt. *a* to *b*,

 $\omega \zeta$ is a curvilinear coord. along segment

- So that $\int_{\partial \Omega \sigma(t)} \sigma \kappa v_i n_i dA = \int_a^b \sigma v_i s_{i,\zeta} d\zeta$
- Integrating by parts, noting that $v_{i,\zeta} = v_{i,j} s_j$, $\int_{\partial\Omega\sigma(t)} \sigma \kappa v_i n_i dA = -\int_a^b \sigma v_{i,j} s_i s_j d\zeta + (\sigma v_i s_i)_a^b$

Moving Mesh

- Account for moving mesh by adding another term to RHS of Stokes' problem:
 ∫_{Ω(t)} v_i (u_i w_j), dV = ∫_{Ω(t)} v ∇ · (u w) dV = (v, ∇ · (u w)) where w is the mesh velocity
- The mesh velocity provides for nodal coords. to be updated as $d\mathbf{x}_{node}/dt = \mathbf{w}$

Results

- Free surface, initially sinusoidal in shape
- Then allowed to vary according to differences in initial fluid pressure compared to that above the free surface
- Free surface gradually began to move and be reshaped by the pressure imbalance



At dimensionless t=0.8, 200th time step; fluid pushing up the middle...

K=32 elements, N=5th order



At dimensionless *t*=1.6, 400th time step; appears to be flattened but fluid still pushing up, vortex pair forming near free surface...



At dimensionless t=2.4, 600th time step; appears to be flattened but fluid pushed to sides at top, twin vortices moved down...



At dimensionless t=3.2, 800th time step; not flattening but seeming to be reversing shape like an oscillating free surface; vortex pair back up...



At dimensionless t=6.4, 1600th time step; not oscillating shape but free surface breaking up; vortices broken up \Rightarrow then numerical instability



At dimensionless t=0.8, 200th time step; Finer mesh shows the same thing but with better resolution: K=64, N=5



At dimensionless t=0.8, 200th time step; But isobars show pressure gradient oscillating w/free surface



At dimensionless t=24, 6000th time step; Finer mesh better details breakup



At dimensionless t=24, 6000th time step; Finer mesh better details breakup & accompanying pressure distortions

Shape-Changing Wall

- Free surface was replaced with a compliant wall that starts with a sinusoidal shape but that shape varied sinusoidally with time as well.
- The fluid response contained regions where the flow-field showed fluid circling up into the high points of the sinusoidal-shaped wall and down from the lower points.
- There appeared vortices oscillating with the oscillating wall

Moving wall

- Non-time-varying sinusoidal-shaped wall given a prescribed vertical velocity downward into the fluid region,
- The fluid moved out through an unconstrained end.
- However, fluid became entrapped under a hump of the sinusoidal shape.
- The simulation could not continue further beyond the point where the non-compliant sinusoidal-shaped wall reached the bottom of the fluid region

Conclusion

- The results obtained suggests that a compliant wall can have its shape altered by the fluid region it bounds and the reverse
- The results also show how the wall can determine where fluid can flow and the way that flow occurs

Future Work

- More combinations planned
- Extend to 3D
- Apply to carotid artery
- Extend SEM potential w/parallel numerical libraries w/solvers, pre-conditioners, etc.

Thanks to

- Dr. Linda Phaire-Washington for opportunity to be Faculty and Student Team (FaST).
- US Department of Energy (DOE), Argonne National Laboratory, MCS Division.
- National Science Foundation and Dr. Hicks, via Louis Stokes Alliance for Minority Participation (LS-AMP or Chicago AMP, ChAMP) program through Chicago State University (CSU) under Dr. Leroy Jones, for their support.